

# Simple algorithm for the correction of MRI image artefacts due to random phase fluctuations

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## Purpose:

Fast Field-Cycling MRI<sup>1</sup> (FFC-MRI) is a novel MRI technique in which the external magnetic field is switched during the imaging experiment. By doing this, FFC-MRI grants access to information which is invisible to conventional MRI scanners, including the variation of  $T_1$  with magnetic field. These measurements, known as  $T_1$ -dispersion, exhibit great promise as a new form of endogenous image contrast, and may have application in the early diagnosis of a range of diseases including osteoarthritis<sup>2</sup>, cancer and neurodegeneration.

In our system, the use of a resistive magnet to perform field-cycling means that the  $B_0$  field is subject to a slow drift with a corresponding drift in frequency. Even when this drift is controlled using an NMR lock or a current feedback loop, small off-resonant effects persist. This results in small discontinuities in k-space, which manifest as ghosting in the phase-encode direction.

Here we present a post-processing technique which is able to correct these ghosts and recover the original image with no prior knowledge of the field-drift.

## Methods:

The magnet (Tesla Engineering Ltd, Storrington, UK) is of a resistive design and is driven by 18 current amplifiers (IECO, Helsinki, Finland). The main magnetic field is set and controlled by a 16-bit, high-precision DAC which provides a field resolution of 3  $\mu$ T. This limits real-time field corrections to 3  $\mu$ T, or approximately 125 Hz, which is sufficient to prevent severe off-resonance effects but still results in ghosting artefacts.

We therefore developed a post-processing algorithm using MATLAB 2014a (Mathworks, Natick MA USA) to attempt to correct the phase errors. The algorithm takes the form of an iterative method inspired from similar techniques for correcting motion artefacts<sup>3,4</sup>. As a minimisation criteria we used the image background; an image with no ghosting should have minimal background signal.

During each iteration the algorithm estimates the phase correction for every line of k-space using a sequential programming (SQP) method, the image is reconstructed and the background signal is estimated. The algorithm terminates once the background signal has converged. Constraints were added on the SQP search in order to null the 1<sup>st</sup> order moment of the phase correction to prevent translation along the phase-encode direction.

The algorithm was tested in simulations, on phantoms and in-vivo. For the simulations we used the Monte-Carlo method: a 128x128 artefact free gradient-echo image was used as the base for 1000 test images with randomly added noise, phase scatter and amount of background area.

## Results

For the Monte-Carlo simulations none of the images failed to converge. Figure 1(a) shows the reference image while (b) shows the same image following the addition of random phase errors, and (c) shows the difference between the original and the corrected image. Figure 1(d) shows the agreement between the phase correction recovered by the algorithm and the ground truth error applied to the original image. The average reconstruction time for a 128x128 image was 7 s on a desktop i5 processor. The processing time follows a square relationship with the matrix size; upscaling the image to 512x512 increased the processing time to 104 s. Superior time efficiency can be realised by parallelising the corrections for multi-dimensional data.

Experimental data from phantom (Figure 2) and in-vivo (Figure 3) imaging reconstructed using the algorithm demonstrate excellent results with no visible ghosting.

## Discussion

The algorithm presented here has demonstrated that artefact free images can be obtained on our FFC-MRI scanner even where there is a drift in resonant frequency without excessive post-processing time. So far we have only tested the algorithm on Cartesian sampled data, however the algorithm should be applicable to other sampling strategies. We have tested the algorithm only to correct the phase errors resulting from the frequency drift of our magnet, but it would be interesting to investigate applications for other types of artefact such as motion.

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3. Atkinson, D. *et al.* Automatic correction of motion artifacts in magnetic resonance images using an entropy focus criterion. *IEEE Transactions on Medical Imaging*, **16**, 903–910 (1997).
4. McGee, K. P. *et al.* Image metric-based correction (autocorrection) of motion effects: analysis of image metrics. *Journal of Magnetic Resonance Imaging*, **11**, 174–81 (2000).

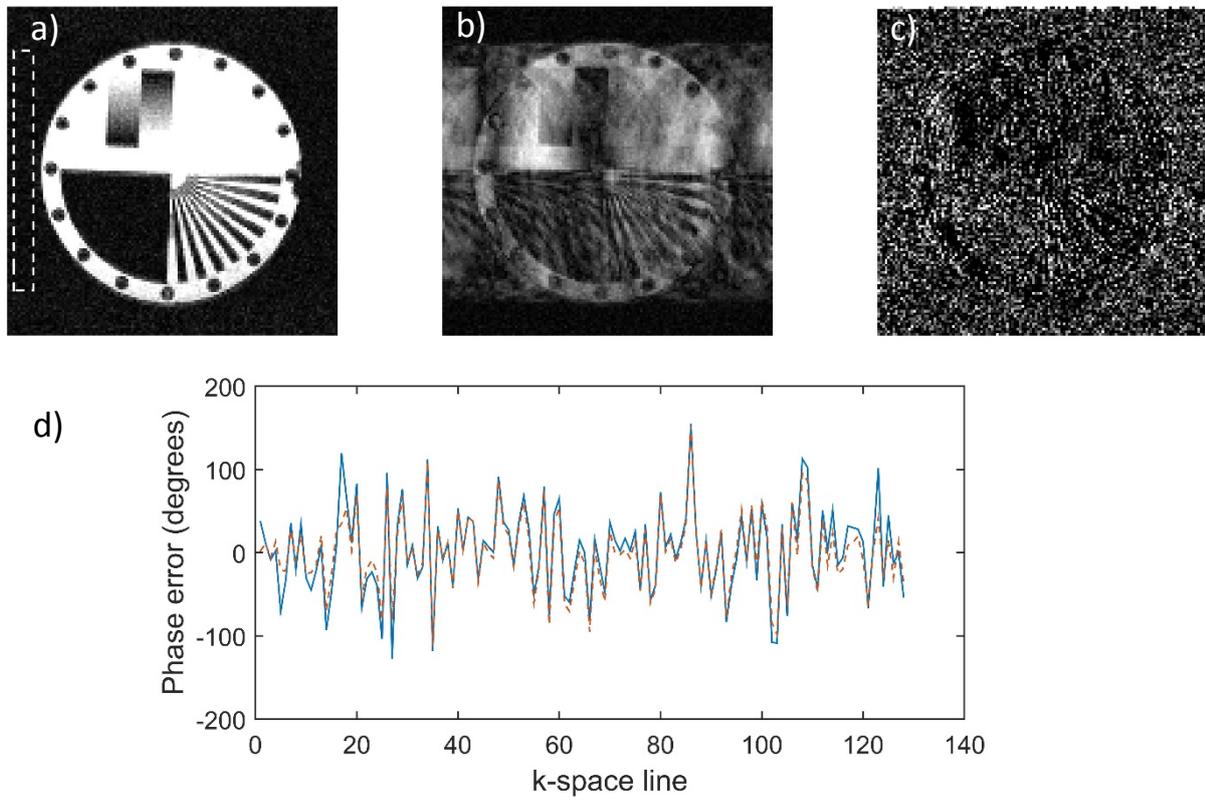


Figure 1: (a) Reference image used for the Monte-Carlo simulations with a region of background highlighted, (b) the image following the addition of random-phase errors to simulate the effects of a resonant frequency drift, (c) difference image of the reference the corrected image following post-processing.(d) shows the agreement between the applied phase errors (red) and the estimated errors (blue).

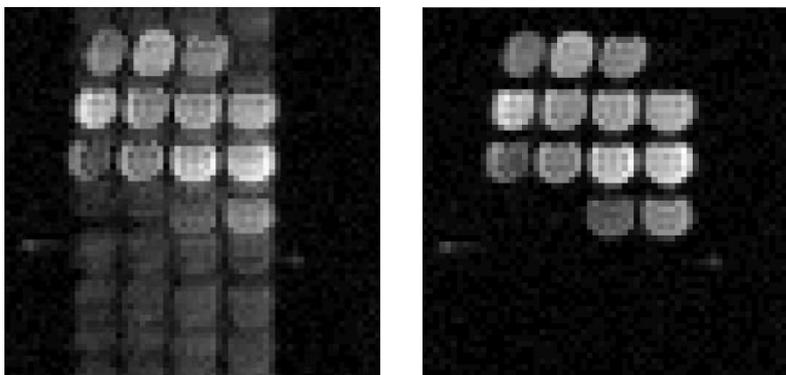


Figure 2: (left) Image of a phantom array prior to correction, showing severe ghosting in the phase-encode direction. (right) The same data set following post-processing showing no visible ghosting

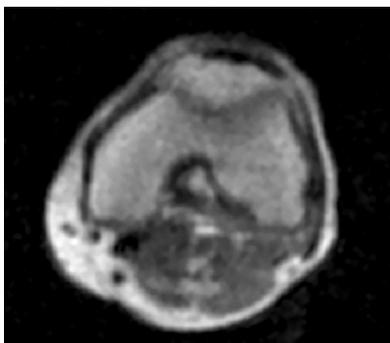


Figure 3: In-vivo spin-echo image of a volunteer's knee following post-processing and showing no artefacts